

# In-situ Monitoring of Biomaterials in Fretting-Corrosion Couples

A. R. Beadling<sup>1)\*</sup> and J. Qi<sup>2)</sup> and M. Rainforth<sup>2)</sup> and M. G. Bryant<sup>1)</sup> and A. Neville<sup>1)</sup>

<sup>1)</sup>Institute of Functional Surfaces, University of Leeds, UK

<sup>2)</sup>Department of Materials Science and Engineering, University of Sheffield, UK.

\*Corresponding author: a.r.beadling@leeds.ac.uk

Common biomaterials used in total joint replacement were investigated under a fretting-corrosion contact such as is found in modular tapers. The tribocouples were monitored using live in-situ sensing to assess degradation during sliding. Changing the fretting regime from ‘stick’ to ‘gross-slip’ resulted in increased acoustic emission hit detection and nanocrystallisation at the surface of the material. Under ‘stick-slip’ however subsurface cracking was observed in the sample; coupled with even higher hit counts. Quantification of AE signals could lead to further understanding in how energy is dissipated in such contacts and the formation of surface tribolayers.

**Keywords:** fretting, tribocorrosion, biomaterials, modular tapers

## 1. Introduction

Fretting-corrosion contacts in joint replacement modular taper operate under different regimes due to the transient nature of biomechanics and biomedical device geometry. These regimes are characterised by a fretting loop and can either be closed in a ‘stick’ regime, partially open in ‘stick-slip,’ or fully opened in ‘gross-slip’ [1]. The area inside the loop is known as the dissipated energy (DE) and is a measure of the work done to the surface (force x displacement). The DE can be related to other in-situ sensing technologies to further understand the degradation, subsurface changes and evolution of tribolayers in such contacts [2].

## 2. Methods

### 2.1. Fretting Rig

A custom fretting tribometer was used to articulate a 25 mm radius domed CoCrMo alloy pin against a Ti-6Al-4V plate; common biomaterials employed in THR. The samples were placed in a bath of foetal bovine serum diluted to 30 g/L total protein content with phosphate buffered saline. A load was selected to give a nominal contact pressure of 300 MPa and the tribo-couples were articulated at varying fretting amplitudes: 10, 25, 50 and 100  $\mu\text{m}$ . This was done in order to capture a range of fretting regimes.

### 2.2. In-situ sensors

The fretting rig was fitted with in-situ sensors in order to monitor the surface degradation in real time. Force and displacement sensors were used to capture the fretting loop data. A three-electrode cell was used to monitor corrosive degradation whereby the pin and plate tribo-couple formed the working electrode. An Acoustic Emission (AE) sensor was also secured to the underside of the plate to record signal data from tribologically induced deformation.

### 2.3. Surface Analysis

After testing, a 10  $\mu\text{m}$  surface cross-sectional slide was taken from within the wear scar in a focused ion beam (FIB) SEM. These slides were then investigated using NanoMEGAS TEM orientation imaging in order to map and quantify subsurface changes to the alloy articulating surface.

## 2.4. Results

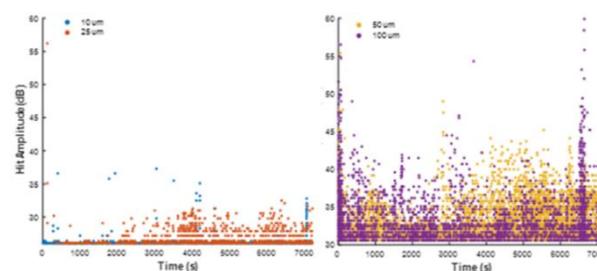


Figure 1: AE Hit Amplitude data for fretting couples at various amplitudes.

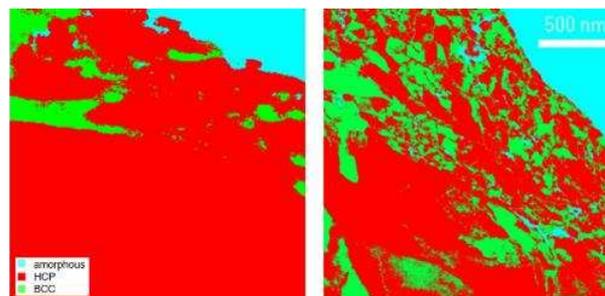


Figure 2: TEM from within the wear scar at 25  $\mu\text{m}$  (left) and 100  $\mu\text{m}$  (right).

## 3. Discussion

The corrosive degradation was found to scale with the fretting amplitude as the regime changed. Moving into ‘gross-slip’ increased DE was coupled with increased AE hit detection and subsurface nanocrystallisation. Under ‘stick-slip’ however lower levels of subsurface change were noted despite even higher levels of AE hit detection. This was explained by observed subsurface cracking; suggesting AE can help quantify different pathways of energy dissipation in-situ.

## 4. References

- [1] Vingsbo, O. and Soderberg, S, “On fretting maps,” *Wear*, 126, 2, 1988, 131-147.
- [2] Baxmann, M. et al., “Biomechanical Evaluation of the Fatigue Performance, the Taper Corrosion and the Metal Ion Release of a Dual Taper Hip Prosthesis under Physiological Environmental Conditions,” *Biotribology*, 12, 2017, 1-7.